

Self-Assembly of a Simple Membrane Protein: Coarse-Grained Molecular Dynamics Simulations of the Influenza M2 Channel

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ABSTRACT The transmembrane (TM) domain of the M2 channel protein from influenza A is a homotetrameric bundle of α -helices and provides a model system for computational approaches to self-assembly of membrane proteins. Coarse-grained molecular dynamics (CG-MD) simulations have been used to explore partitioning into a membrane of M2 TM helices during bilayer self-assembly from lipids. CG-MD is also used to explore tetramerization of preinserted M2 TM helices. The M2 helix monomer adopts a membrane spanning orientation in a lipid (DPPC) bilayer. Multiple extended CG-MD simulations ($5 \times 5 \mu\text{s}$) were used to study the tetramerization of inserted M2 helices. The resultant tetramers were evaluated in terms of the most populated conformations and the dynamics of their interconversion. This analysis reveals that the M2 tetramer has $2 \times$ rotationally symmetrical packing of the helices. The helices form a left-handed bundle, with a helix tilt angle of $\sim 16^\circ$. The M2 helix bundle generated by CG-MD was converted to an atomistic model. Simulations of this model reveal that the bundle's stability depends on the assumed protonation state of the H37 side chains. These simulations alongside comparison with recent x-ray (3BKD) and NMR (2RLF) structures of the M2 bundle suggest that the model yielded by CG-MD may correspond to a closed state of the channel.

INTRODUCTION

Membrane proteins comprise $\sim 25\%$ of most genomes, and in humans are a major target for drugs (1,2). Yet of the $\sim 47,000$ structures deposited in the Protein Data Bank (3), only ~ 300 are for membrane proteins, corresponding to <150 unique structures (http://blanco.biomol.uci.edu/Membrane_Proteins_xtal.html). Thus, despite the progress made in determining membrane protein structures (4), it is of some importance to develop methods that enable prediction of membrane protein structures either ab initio or as an adjunct to methods for determining low-resolution structures (5).

Models of membrane protein folding suggest that it may occur via two major stages (6–9). First, upon insertion into the bilayer, the polypeptide forms independently stable transmembrane (TM) α -helices. Second, these TM helices subsequently pack together to form the tertiary structure of the protein. Subsequent to and/or in parallel with the initial insertion phase, TM helices can start to seek out their most stable native conformations. This search for the native protein conformation may include the reorientation of the helices from their original insertion positions to alignments that will lead to the most stable packing arrangement of the helices. This search may itself proceed via several steps. For example,

bacteriorhodopsin has several folding intermediates (10), and indeed there may exist multiple folding pathways leading to the native structure (11), consistent with the more general concept of protein folding on a funnel-shaped energy landscape (12).

Recent studies with small water-soluble proteins suggest that molecular dynamics (MD) and Monte Carlo simulations can be used to explore aspects of protein folding (13). For example, simulation folding studies on small soluble peptides, e.g., Trp cage (14,15), yielded predicted structures with an accuracy close to that of NMR. However, Trp cage folds in ~ 10 ns, whereas the folding and assembly of small membrane peptides occurs on the microsecond timescale (16), i.e., beyond the range of most atomistic MD simulations of membrane systems (17–19). However, coarse-grained (CG) approaches, in which small groups of atoms are treated as single particles, allow one to expand the length of MD simulations of membranes to tens of microseconds (20–30). Recent works have adapted CG lipid models for use with proteins (27,28,31–33), and demonstrated that CG-MD may be used to simulate, e.g., the self-assembly of TM helix dimers of the simple model membrane protein glycophorin A (31) and the folding of a TM α -helical hairpin (28).

The M2 channel protein from influenza A virus (Fig. 1) provides a good test case for modeling studies of simple membrane proteins (34,35). It is a 97-residue protein containing a single TM α -helix. The protein exists as a tetramer, with the ion channel formed by a parallel bundle of four TM helices. M2 has been the subject of extensive experimental (36–58) and computational (59–65) studies in the past few years. In particular, it has been used in simulations based on an implicit membrane and solvation model to study folding/self-assembly of the TM helix tetramer (64,65). It therefore provides a well-

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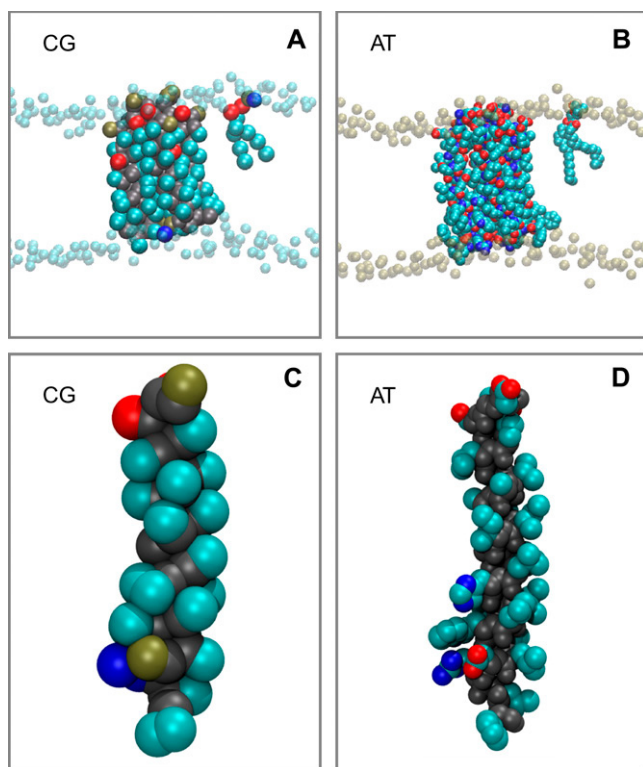


FIGURE 1 CG (A) and atomistic (B) systems, with the M2 tetramer, one DPPC lipid molecule, and the phosphate particles/atoms of the remaining DPPC molecules represented. Colors for the atoms: cyan, carbon; red, oxygen; blue, nitrogen; and bronze, phosphorous. Colors for CG particles: cyan, apolar; red, polar; blue, positively charged; and bronze, negatively charged. The CG (C) and atomistic (D) single M2 helices are shown using the same color schemes, although the atomistic backbone has been colored gray for clarity.

documented test case for analysis of TM helix bundle self-assembly and dynamics using CG-MD. Furthermore, two recent structures of the M2 TM helix tetramer, as revealed by x-ray crystallography in the presence of detergent (octyl glucoside) (66) and by NMR in detergent (DHPC) micelles (67), enable the model structures to be compared with those determined experimentally, albeit in different environments.

In this study, CG-MD simulations are used to study the partitioning of isolated TM helices into a lipid bilayer during self-assembly of a bilayer. CG-MD is also used to explore the self-assembly of a tetrameric bundle of M2 TM helices in a bilayer, and the conformational dynamics of the resultant helix bundle. The resultant M2 bundle model is converted from CG to atomistic (AT) form and shown to be stable in ~ 15 ns duration simulations in an atomistic lipid bilayer.

METHODS

M2 TM helix and bilayer models

A 27-mer peptide (residues D²¹SSDPLVVAASIIIGLHLILWILDRLF⁴⁷) was used to model the TM region of M2 plus several residues on either side (68). This region was chosen on the basis of experimental evidence (69,70) in

combination with results of a TM helix prediction server (71). Modeller v7.7 (72–74) was used to create a structure with an α -helical region for the proposed TM domain (residues 22–46) with an additional residue at either end in a random coil conformation. This atomistic model was converted to CG using the protocol described previously (31). The result was a monomer 27 amino acids in length, with the central 25 amino acids held together in a comparatively rigid α -helical structure. Since the CG backbone particles cannot form hydrogen bonds, harmonic restraints were used to maintain the α -helical conformation.

To simulate bilayer formation and partitioning of a single TM helix into the membrane, a simulation box (of dimensions $100 \times 100 \times 100 \text{ \AA}^3$) containing the CG α -helical peptide was filled with 256 randomly placed and orientated CG dipalmitoylphosphatidylcholine (DPPC) lipids, ~ 3000 CG water particles, and four CG Na⁺ ions. This primary simulation resulted in a stable membrane-spanning M2 TM helix (see Fig. 2). This monomeric helix was replicated to produce four monomers of similar orientation, which were inserted into a preformed and equilibrated CG DPPC bilayer, $\sim 45 \text{ \AA}$ apart from one another. This system was the basis of five subsequent tetramer simulations, each of $5 \mu\text{s}$ duration.

CG simulation parameters and protocols

All simulations were performed using GROMACS (www.gromacs.org) (75,76). CG simulations were performed as described by Bond and Sansom (31). The CG parameters for lipids (DPPC), ions, and water molecules were as described by Marrink et al. (21). The CG parameters for amino acids were a modified version of that described by Bond and Sansom (31), and the same as that described by Bond et al. (28) and Bond and Sansom (32). Briefly, a CG peptide model was generated from the atomistic model, yielding a chain of backbone particles with attached side-chain particles. Interparticle bond potentials used a force constant of $50 \text{ kJ mol}^{-1} \text{ \AA}^{-2}$. The equilibrium bond length was 3.6 \AA for the backbone particles. Different amino acids had different equilibrium bond length(s) for their side-chain particle(s). Harmonic restraints were applied between backbone particles to mimic secondary structure H-bonds in the atomistic structure. The target distance was 6 \AA , with a force constant of $10 \text{ kJ mol}^{-1} \text{ \AA}^{-2}$.

For all CG simulations, Lennard-Jones interactions were smoothly shifted to zero between 9 \AA and 12 \AA , and electrostatics were smoothly shifted to zero between 0 \AA and 12 \AA , with a relative dielectric constant of 20 used for explicit screening. The nonbonded neighbor list was updated every 10 steps. All simulations were performed at constant temperature, pressure, and number of particles. The temperatures of the protein, DPPC, and solvent were each coupled separately using the Berendsen algorithm (77) at 323 K , with a coupling constant $\tau_T = 1 \text{ ps}$. The system pressure was anisotropically coupled using the Berendsen algorithm at 1 bar with a coupling constant $\tau_P = 1 \text{ ps}$ and a compressibility of $5 \times 10^{-6} \text{ bar}^{-1}$. The time step for integration was 40 fs , and coordinates were saved every 400 ps for subsequent analysis. Analyses were performed using GROMACS tools and locally written code. Visualization used VMD (78).

Atomistic simulations

Atomistic simulations used an extended united atom version of the GROMOS96 force field (79,80). All energy minimizations used <1000 steps of steepest descents to relax any steric conflicts generated during setup. Long-range electrostatic interactions were treated using the particle mesh Ewald method (81) with a 10 \AA cutoff for the real space calculation. A 10 \AA cutoff was used for the van der Waals interactions. All simulations were performed in the constant number of particles, pressure, and temperature (NPT) ensemble. The temperatures of the protein, lipids, water, and ions were coupled separately using the Berendsen thermostat (77) at 323 K with a coupling constant $\tau_T = 0.1 \text{ ps}$. The pressure was coupled semiisotropically using the Berendsen barostat at 1 bar with coupling constant $\tau_P = 1 \text{ ps}$. The time step for integration was 2 fs . The LINCS algorithm (82) was used to restrain bond lengths.

General analysis

Simulation results were analyzed using GROMACS tools and locally written code. The clustering of tetramer structures was carried out using NMRclust (83). Secondary structure analyses used DSSP (84). Pores within the helical bundle were analyzed and visualized using HOLE (85). Visualization used VMD (78).

RESULTS

M2 helix partitioning into a lipid bilayer

The initial set of simulations (CG-M1 to CG-M10) consisted of self-assembly simulations starting from a box of randomly positioned lipids plus a single 27-mer M2-TM peptide in an α -helical conformation (Table 1). The aim of the simulation was to test the assumption of a preferred TM orientation of the M2 peptides. For 90% of the simulation time, as the lipids self-assemble into a bilayer, the peptide helix partitions into the bilayer and remains spanning it (Fig. 2). This occurs after an average of ~ 25 ns, after which time both the bilayer and membrane-spanning helix remain stable throughout the remainder of the simulation. It should be noted that the dynamics of CG simulations may be faster than that of a corresponding AT simulation, with a 3–6-fold speed-up factor depending on the molecules in question (21). Thus from 75 to 150 ns of “atomistic time” was needed for bilayer/helix self-assembly. This is comparable to the estimate of 50–100 ns obtained from earlier atomistic simulations, albeit on a smaller system (86).

The tilt angle of the helix in the TM orientation simulations relative to the bilayer normal (i.e., the z axis) has an average of $16^\circ (\pm 7^\circ)$. The N-terminal of the M2 TM helix contains several charged and polar residues (D21, S22, S23, and D24), whereas the C-terminal contains both charged and aromatic residues (R45 and F47). These residues interact with the lipid headgroups and appear to act as anchors of the helix in the membrane.

Thus, this relatively simple CG-MD simulation is consistent with both experimental studies (36,87) and implicit bilayer simulations (64,88) indicating that the M2-TM helix adopts a membrane-spanning orientation.

M2 TM helix tetramerization

Five independent self-assembly simulations of the influenza M2 tetramer (CG-T1 to CG-T5; see Table 1), each of duration $5 \mu\text{s}$, were performed, starting from four isolated M2-TM helices inserted in a parallel fashion and similar orientation (at an interhelix separation of $\sim 45 \text{ \AA}$) in a preformed DPPC bilayer. Thus, this simulation mimics the second stage of membrane protein folding, i.e., oligomerization and packing together of the helices. The formation of helix bundles was assessed by monitoring the distances between the centers of mass of the Ca particles of the various pairwise combinations of helices as a function of time (Fig. 3).

In each of the five simulations a tetrameric bundle was formed. It can be seen that this occurs by initial formation of

TABLE 1

Simulation	Setup	Duration (ns)
CG-M1 to CG-M10	27-mer M2-TM peptide, 256 DPPCs, ~ 3000 water particles, 4 Na^+ ion particles	10×1000
CG-T1 to CG-T5	$4 \times$ 27-mer M2-TM peptides, preequilibrated bilayer (195 DPPCs), ~ 3000 water particles, 16 Na^+ ion particles	5×5000
CG-T6	$4 \times$ 27-mer M2-TM peptides (randomly orientated) in a preequilibrated bilayer (196 DPPCs), ~ 3000 water particles, 16 Na^+ particles	5000
CG-T ⁺	$3 \times$ 27-mer M2-TM peptide with neutral H37, 1 \times 27-mer M2-TM peptide with positive H37, preequilibrated bilayer (195 DPPCs), ~ 3000 water particles, 14 Na^+ particles	5000
CG-T ²⁺	$2 \times$ 27-mer M2-TM peptide with neutral H37, 2 \times 27-mer M2-TM peptide with positive H37, preequilibrated bilayer (195 DPPCs), ~ 3000 water particles, 12 Na^+ particles	5000
CG-T ³⁺	1 \times 27-mer M2-TM peptide with neutral H37, 3 \times 27-mer M2-TM peptide with positive H37, preequilibrated bilayer (195 DPPCs), ~ 3000 water particles, 10 Na^+ particles	5000
CG-T ⁴⁺	$4 \times$ 27-mer M2-TM peptide with positive H37, preequilibrated bilayer (195 DPPCs), ~ 3000 water particles, 8 Na^+ particles	5000
AT-T ⁰	$4 \times$ 27-mer M2-TM peptides, preequilibrated bilayer (195 DPPCs), ~ 8000 water molecules, 8 Na^+ ions	15
AT-T ⁴⁺	$4 \times$ 27-mer M2-TM peptides, preequilibrated bilayer (195 DPPCs), ~ 8000 water molecules, 4 Na^+ ions	15
CG-x-ray	$4 \times$ 25-mer (x-ray-to-CG*), preequilibrated bilayer (203 DPPCs), ~ 3000 water molecules, 8 Na^+ ions	500
CG-D4	$4 \times$ 25-mer (AT model-to-CG [†]), preequilibrated bilayer (203 DPPCs), ~ 3000 water molecules, 8 Na^+ ions	2000

*For this simulation, the crystal structure was converted into a CG model.

[†]For this simulation, the D4 model adapted from the crystal structure was converted into a CG model.

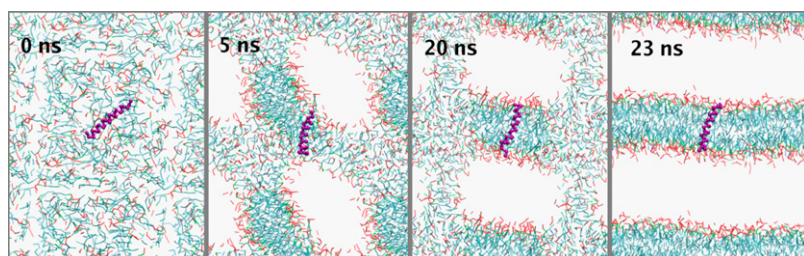


FIGURE 2 Snapshots of the system during the bilayer-forming simulation, showing the helix partitioning into the bilayer as it forms (water particles omitted for clarity). The helix partitions into the arranging lipids that form a stable bilayer after ~ 23 ns. This bilayer remains intact (and the helix continues to span the bilayer) for the remainder of the simulation.

dimer, which subsequently grows by addition of helices until the tetramer is formed. Averaging across the five simulations, the mean time taken for formation of a tetramer was 550 ns (± 120 ns). It is worth noting that in each simulation a loose tetrameric assembly formed within a shorter period of time; the mean time quoted is for formation of a plausible homo-tetrameric left-handed helix bundle. However, to allow equilibration of each bundle before analysis, only data from 1 μ s onward were considered, giving 4 μ s per simulation and 20 μ s of tetramer simulation time in total.

Conformation of the four-helix bundle

The five simulations were each clustered (using NMRclust (83)) on their $C\alpha$ RMSDs to yield representative frames from the three top clusters per simulation. A comparison of the 15 structures, via calculation of a $C\alpha$ RMSD matrix, yielded

four major conformations, combinations of which were present in all of the simulations. Furthermore, a more detailed examination of these four major conformations revealed that they corresponded to the same structure, but with different numbering (i.e., permutation) of the helices. Manual re-numbering of the helices resulted in a single cluster of structures (see Fig. 4) with an overall $C\alpha$ RMSD of 3 Å between one another. Note that this is comparable to, e.g., the RMSD of an NMR ensemble structure for the TM domain of the F1F0 ATPase c-subunit (89).

Previous modeling studies of M2 have assumed fourfold rotational symmetry (44,61,65) for the tetramer, such that the two diagonal distances across the bundle (distances H1-H2 and H3-H4 in Fig. 5) are by definition equal to one another. However, in the final ensemble of 11 structures (four structures having been excluded during the clustering as outliers/minor conformations) of the tetramer, the two average diagonal distances are 11.5 ± 0.3 Å and 16.8 ± 0.2 Å. Thus,

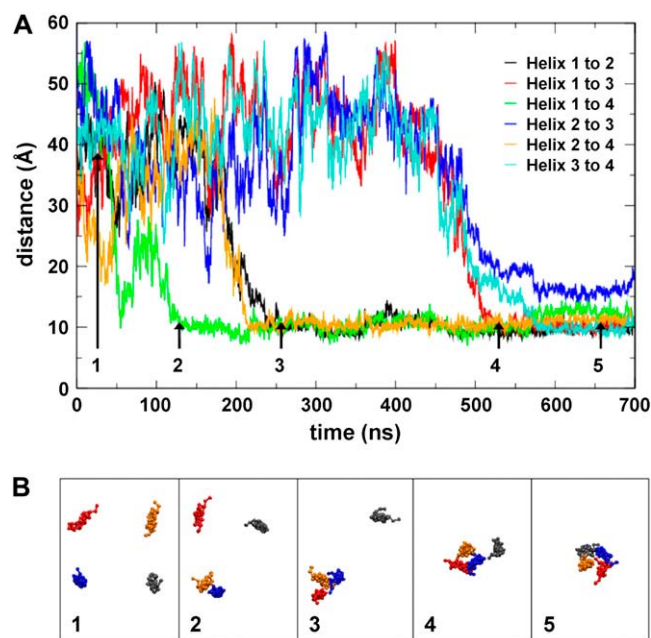


FIGURE 3 Distances between the centers of mass of the helices as they aggregate together into a tetramer (A), and snapshots of the positions of the helices (B) as tetramerization takes place. Helix 1, blue; helix 2, red; helix 3, gray; and helix 4, orange. This indicates that helices 1 and 4 form a dimer after ~ 120 ns, which becomes a trimer (with helix 2) ~ 100 ns later. A four-helix aggregate is formed after ~ 530 ns, which then rearranges into a left-handed helix bundle.

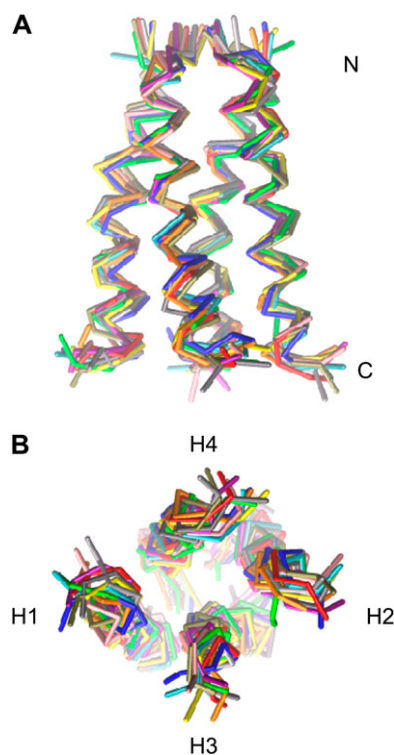


FIGURE 4 Ensemble represents conformations 1–4 rotated by 90° , 180° , or 270° so that they can all be superimposed upon one another.

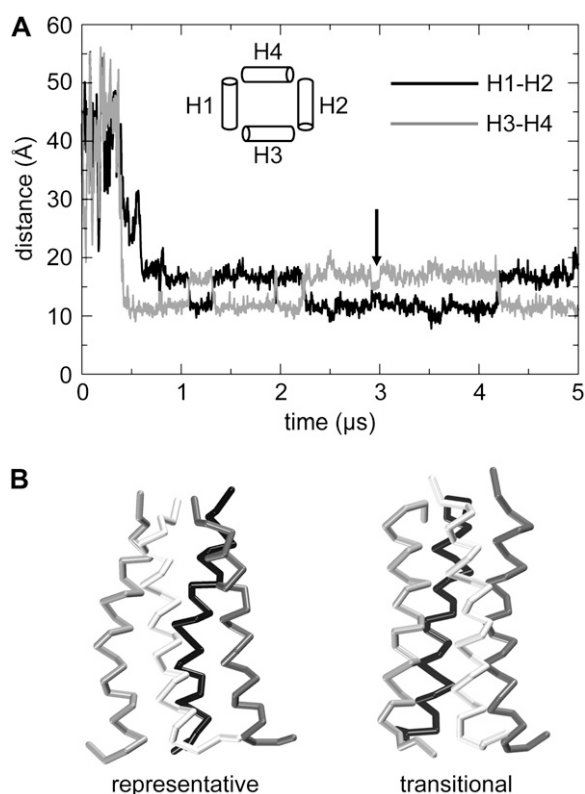


FIGURE 5 (A) Helix distances show that helices 1 and 2, and helices 3 and 4 are opposite each other in the arrangement of the helical bundle. It can be seen that at several points the two diagonal distances “switch” so that the closer helices move apart, whereas the distant helices approach one other. (B) Comparison of 2 \times -symmetrical (“representative”) and 4 \times -symmetrical (“transitional”) M2 helix bundle structures.

the ensemble structure shown in Fig. 4 has 2 \times rotational symmetry. Interestingly, such symmetry has been seen in some atomistic simulations of M2 models (90).

From visual inspection, the helix bundle is clearly left-handed, in agreement with previously published data (36). During the simulation, the average tilt angle of the helices is $16^\circ \pm 7^\circ$. This result is comparable to some experimental estimates of the tilt angle ($14^\circ \pm 5^\circ$ (91)), but somewhat less than other findings ($33^\circ \pm 3^\circ$ (36), $37^\circ \pm 3^\circ$ (40), $32^\circ \pm 6^\circ$ (87)). Although there appears to be a discrepancy between the calculated tilt angle for the CG system and some other experimental data, it is worth noting that these experiments were carried out in DMPC (36,40,87), whereas the CG-MD simulations presented here utilized DPPC, which would be expected to result in a ~ 4 Å thicker hydrophobic core than in a DMPC bilayer (92). However, it should be mentioned that due to the granularity of the CG lipid model, the CG-DPPC molecule in our simulations represents lipid tails of 14–18 carbons in length (21,33). Despite this, however, our simulations reveal a bilayer thickness (defined by the phosphate–phosphate distance) of ~ 39 Å, which more closely resembles the corresponding distance in DPPC (37 Å) (93). It might be anticipated that in a wider lipid bilayer the tilt angle will

be lower. Indeed, previous work stated that the conformation of M2 depends on the lipid bilayer environment (55), with a thicker hydrophobic distance resulting in a shallower tilt angle. It is also worth noting that the experimentally derived model that most closely matches the CG simulation ($14^\circ \pm 5^\circ$ (91)) was based on data obtained from M2 channels expressed in *Xenopus laevis* oocytes. Furthermore, the tilt angle in the recent NMR structure in DHPC micelles (67) is $\sim 15^\circ$.

The average crossing angle between sequential helices was calculated at $21^\circ \pm 7^\circ$. This compares well with the experimentally derived model value of 19° (91). The orientation of the helices relative to each other was such that the proposed pore-lining residues (V27, A30, S31, G34, H37, F38, and W41) (91,94,95) are indeed facing the center of the helix bundle. The side-chain particles for the important pore-gating residues, H37 and W41 (see Fig. 6), were also observed to form two rings of constriction within the center of the helix bundle that occluded the pore (see below). In agreement with recent atomistic simulations (96), the V27 region was also seen to form a narrow passage in the pore.

The interhelix distances discussed so far were calculated using the center of mass of all of the backbone particles. Further analysis of the interhelix distance was carried out by dividing the helices into N- and C-terminal segments (where the N-terminus was defined as the center of mass of the backbone particles for the first five residues of the helix, and the C-terminus for the last five residues). The average adjacent (i.e., not diagonal) helix–helix distance for the N-terminus was 9.6 ± 0.1 Å (9.5 Å, 9.4 Å, 9.6 Å, and 9.7 Å for helices 1-3, 3-2, 2-4, and 4-1, respectively), whereas for the C-terminus the corresponding distance was 14.0 ± 0.2 Å (14.1 Å, 14.2 Å, 13.7 Å, and 14.1 Å for helices 1-3, 3-2, 2-4, and 4-1, respectively). Thus the N-terminal segments of the helices are packed more closely together than the C-terminal segments. Again, this seems to agree with available structural data. A further simulation (simulation CG-T6, Table 1) was also run in which the helices were orientated randomly (by random rotations about their bilayer normal axes) in the bilayer. This resulted in the same converged conformation, with representatives being within 2 Å of the central structure of the main ensemble produced from simulations CG-T1 to CG-T5 (Fig. 4).

Thus, overall, the ensemble of bundle structures agrees well with previous structural data, other than in the departure from exact 4 \times rotational symmetry. Indeed, recent x-ray studies of the M2 TM tetramer (66) suggest that local deviations from exact 4 \times symmetry may occur.

Dynamics of the helical bundle

The CG simulations of the tetrameric helix bundle were further analyzed in terms of possible switching between alternative conformations. From analysis of the interhelical distances (Fig. 5), it is evident that switching occurs on a

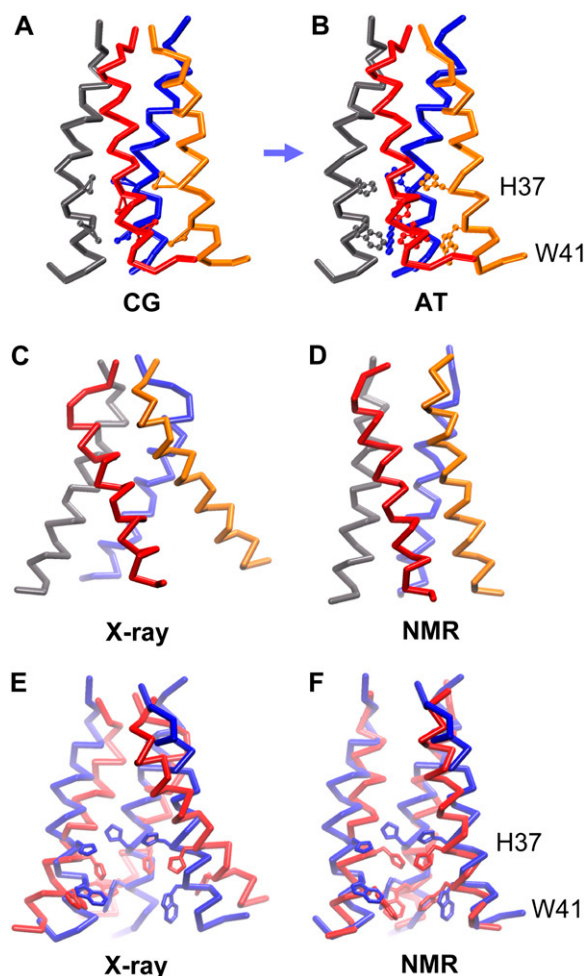


FIGURE 6 Comparison of the CG (A) and atomistic (B) models that was based on the CG structure. The trace of the CG backbone particles and the atomistic α -carbons are represented (helix 1, blue; helix 2, red; helix 3, gray; and helix 4, orange). The side-chain particles for the CG residues H37 and W41, and the heavy atoms of the equivalent atomistic residues are shown in more detail. (C) The x-ray structure (66) and (D) the NMR structure (67) of the M2 TM helix bundle are shown fitted to the converged CG model. E and F show (respectively) the α traces of the x-ray and NMR structures (red) fitted onto our atomistic model (blue) with the H37 and W41 side chains also represented. The nearest helix has been removed from E and F for clarity.

$\sim 1 \mu\text{s}$ timescale between two alternative twofold symmetrical structures. In one of these two conformations, helices H1 and H2 are farthest from each other, whereas in the other the most distant helices are H3 and H4. The distances between these helices versus time (Fig. 5) suggest that these two conformations switch back and forth in a concerted motion, with helices H1 and H2 moving toward each other as helices H3 and H4 move apart. In addition, occasionally a “transitional conformation” between the two is observed (e.g., as indicated by the vertical arrow in Fig. 5). A more detailed examination of this structure suggests that during the transition the average tilt angle of the helices ($\sim 10^\circ$) is less than that during the simulation as a whole ($\sim 16^\circ$).

This decrease in tilt angle helps to accommodate the larger residues (H37 and W41) that face toward the center of the pore. It also appears that as the two $2\times$ -symmetrical conformations switch between one another the transitional bundle is closer to being $4\times$ symmetrical (see Fig. 5B), with less tilted helices such that the overall shape of bundle is less “conical”.

Charge state of the histidine

The two recent experimental structures of M2 have been suggested to represent open (x-ray (66)) and closed (NMR (67)) conformations of the helical bundle. Our initial CG tetramerization simulations (CG-T1 to CG-T5) treated the H37 side-chain particles as neutral. Thus, the model generated most likely corresponds to the proposed closed state. This is in agreement with the better fit of the model to the NMR than to the x-ray structure. To see whether we could simulate the open (or intermediate) states of the channel, we turned the H37 residues into a positively charged side chain by altering the secondary side-chain particle from type Nda (nonpolar) to Qda (charged). Thus systems with one, two, three, and four positively charged H37 side chains were created (CG-T1⁺, CG-T2⁺, CG-T3⁺, CG-T4⁺; see Table 1). Tetramerization of these systems was simulated as described above, and the resultant tetramers were analyzed.

Of interest, it was found that the average tilt of the helices in the bundle did not significantly alter with an increase in the protonation state of the histidine residues. However, it did seem that there were some more subtle changes in the packing of the helices as more of the H37 residues were charged. The conical shape of the converged (H37 neutral) CG M2 tetramer could be defined by the ratio as of the area (A_N) formed by the centers of mass (for each helix) of the five residues at the N-terminus of each monomer to the corresponding area (A_C) formed by centers of mass of the five residues at the C-terminus of each monomer. So, for example, for simulation CG-T3 (all H37 residues neutral) $A_N : A_C = 1:2.1$, whereas for CG-T4⁺ (all H37 residues charged) $A_N : A_C = 1:2.3$, indicating a somewhat wider C-terminal packing when in CG-T4⁺. To explore this further, the area between the centers of mass of the four H37 residues was calculated. For CG-T3 this area was 43 \AA^2 , whereas for CG-T4⁺ this area had almost doubled to 77 \AA^2 . Thus, even at the CG-MD level (which truncates the electrostatic interactions somewhat (21,28)), our model simulations suggest an opening of the M2 channel at the C-terminal mouth as a result of the repulsion of charged H37 residues, which move away from each other via reorientation of the helices without large changes in tilt angle.

Conversion to an atomistic model

To more fully assess the conformational dynamics and stability of the M2 TM tetramer model generated by the CG self-

assembly simulations, the CG structure was converted to an atomistic model, which was then the starting point for conventional atomistic simulations. To convert the CG protein model, Modeller v7.7 (<http://www.salilab.org/modeller/>) was used, with the backbone particles of the CG model as a template for the C α atoms. An ensemble of 1000 models was produced, which was subsequently filtered in terms of RMSD (for the backbone positions and also for key side-chain positions) to yield the atomistic model that best fitted the input CG model. To convert the CG lipid bilayer to an atomistic equivalent, we used a library of 1500 different conformations of DPPC molecules derived from an atomistic simulation of a pure DPPC bilayer. For each CG lipid, the entire library was searched to determine which atomistic conformation provided the best matches (defined via the RMSD of the 12 CG particles against their atomistic equivalents). These AT lipid molecules were then superimposed onto their CG counterparts, and concatenated together with the AT protein model. The resultant AT system was then energy-minimized before solvation and addition of counterions.

The outcome of this conversion procedure is illustrated in Fig. 6, *A* and *B*. The RMSD between the CG protein conformation and the modeled atomistic structure is 1.9 Å (calculated using the CG backbone particles versus the C α atoms plus the side-chain particles against the corresponding side-chain atoms), with a backbone-C α RMSD of 0.7 Å. In particular, it can be seen that the AT model has an overall conical shape, with the side chains of H37 and W41 directed toward the interior of the pore.

The conformational dynamics and stability of the resultant AT model were assessed in a pair of related MD simulations (Table 1 and Fig. 7). In simulation AT-T⁰ the four H37 residues were in their neutral (i.e., unprotonated) state, whereas in simulation AT-T⁴⁺ all four histidines were protonated. Comparing the C α RMSDs for the two simulations (Fig. 7 *A*), it can be seen that the conformational drift is, as anticipated, substantially less for the AT-T⁰ simulation than for the AT-T⁴⁺ simulation. For the AT-T⁰ simulation the C α RMSD after ~15 ns is ~3.5 Å relative to the starting structure. This is comparable to that seen in, e.g., simulations of low-resolution x-ray or EM structures (97). The profile of C α root mean-square fluctuation versus residue (Fig. 7 *B*) suggests that fluctuations in the vicinity of the H37 are low for AT-T⁰, and somewhat higher for AT-T⁴⁺. Significantly, over the 15 ns of the simulations (for both AT-T⁰ and AT-T⁴⁺), the diagonal helix-helix distances (i.e., between H1 and H2, and between H3 and H4) change by <1 Å. Thus, these simulations confirm that switching between the two 2 \times -symmetrical structures (seen in the CG simulations on a ~1 μ s timescale) is not seen on the much shorter timescale of the atomistic simulations.

The atomistic model pore (at $t = 0.25$ ns from AT-T⁰; Fig. 8) was analyzed in terms of the central pore using HOLE (85). Two constrictions to the central pore were observed: one at the N-terminus and one in the vicinity of the H37 side

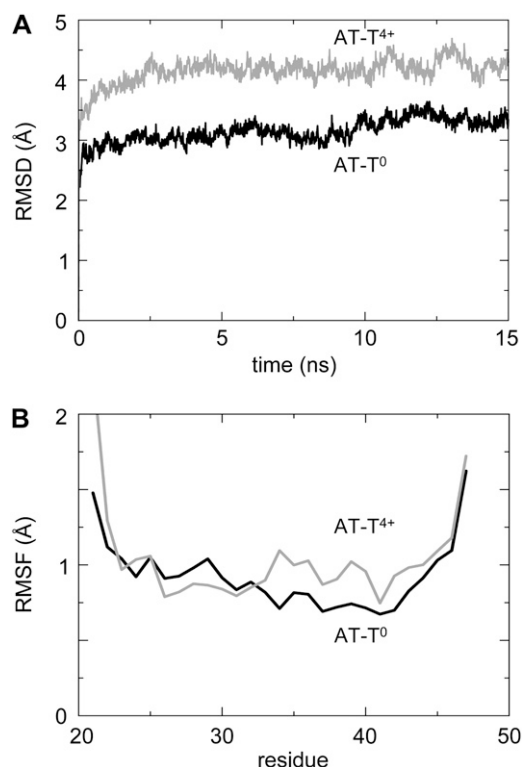


FIGURE 7 RMSD (top) and RMSF (bottom) for the two atomistic simulations containing the histidine-neutral (solid) system and the histidine-4⁺ (shaded) system.

chains, the latter suggesting that this model may correspond to a closed conformation of the channel. A comparable N-terminal constriction is observed in the recently determined x-ray structure (66) and in some recent simulations based on models (e.g., (62,90)). This N-terminal constriction is also in the vicinity of V27, which has been suggested to form an amantadine-sensitive “second gate” (96). A constriction is also seen in the recent NMR structure (67) around the H37 region. The pore radius profile of the atomistic model (see Supplementary Material, [Data S1](#)) shows that whereas the N-terminal region more closely resembles the N-terminal of the x-ray structure, the C-terminal region more closely resembles that of the NMR structure, with a smaller cavity in the center.

This model was also compared with the crystal structure of the M2 TM helix bundle (Fig. 6 *C*) (66). The initial RMSD for the C α atoms of the AT-T⁰ starting conformation against the x-ray structures is relatively high (5 Å) and the corresponding plateau value during the AT-T⁰ simulation was 5.6 Å. The x-ray structure was also compared with the initial CG simulations that were used to form the tetramer (CG-T3 in particular) to see whether the crystal conformation was sampled at any point throughout the CG bundle dynamics. The minimum RMSD observed was 3.9 Å. In a further comparison, the x-ray structure (Fig. 6 *C*) was converted into a CG model and used to initiate a further simulation (CG-x-ray; see Table 1). The D4 model constructed from the x-ray

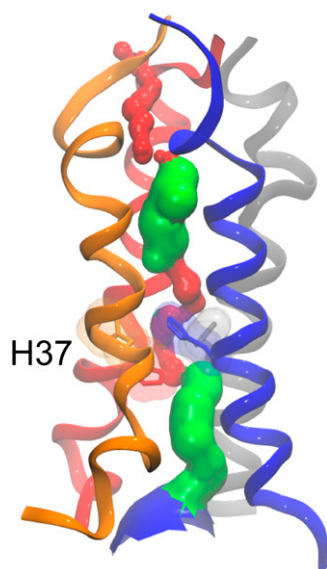


FIGURE 8 Pore profile of the atomistic channel, taken from a snapshot during the histidine-neutral simulation. The side chains of the key gating residues (H37) are shown. The color scheme for the pore surface is as follows: red, radius < 1.15 Å (no water can pass); green, 1.15 Å $<$ radius < 2.30 Å (single-file water); and blue, radius > 2.30 Å (multiple waters). Helix 1, blue; helix 2, red; helix 3, gray; and helix 4, orange.

structure (which is suggested to represent a more closed state of the channel (66)) was also converted to a CG model and used as the initial structure for a subsequent CG-MD simulation (CG-D4; Table 1). The $C\alpha$ RMSD for CG-x-ray after 500 ns was quite high at ~ 6 Å, and the $C\alpha$ RMSD for the CG-D4 simulation also reached a plateau value of ~ 6.5 Å after 500 ns (and subsequently fluctuated about this for the remainder of the simulation). This degree of conformational drift could be attributed to two factors: a degree of collapse of the more “open” regions between the C-termini of the helices, and interhelix movement (the longest interhelix distance switching between H1-H2 and H3-H4, as seen in CG-T1 to CG-T5). It is interesting that in the x-ray structure, two β -octyl glucoside molecules seem to help hold the C-termini of the helices open. To evaluate whether this collapse of the structure had resulted in convergence of the CG-x-ray simulation with the bundle orientation formed from the CG-T3 simulation, an RMSD matrix between the two simulations was calculated. During some limited regions a degree of convergence (< 4 Å) was seen (a similar trend, but to a lesser extent, was seen for the CG-D4 simulation).

DISCUSSION

In this study we have demonstrated that an ensemble of $5 \mu\text{s}$ CG-MD simulations may be used to self-assemble a four-TM helix bundle, i.e., the influenza M2 ion channel TM helix tetramer. Furthermore, this approach yields a converged structure for the M2 TM helix bundle in a lipid bilayer. The

resultant model of the M2 TM bundle is compatible with the majority of the available structural, mutational, and biophysical data. A novel aspect of the CG-MD simulations is that the converged model shows $\sim 2\times$ rotational symmetry, rather than the exact $4\times$ symmetry assumed in many previous modeling and structural studies. The M2 helix bundle undergoes a concerted switching motion between two related $2\times$ -symmetrical structures on a $\sim 1 \mu\text{s}$ timescale. Conversion of the CG to an AT model yielded a structure that was stable in 15 ns duration AT-MD simulations. As expected, the conformational switching seen in the CG-MD simulations was not seen in the (substantially shorter timescale) AT-MD simulations.

To test the sensitivity of the CG simulations to changes in the sequence of the M2 helix, self-assembly simulations (data not shown) were performed in which the sequence of the M2 TM peptide was scrambled. Simulations on this helix resulted in partitioning into the bilayer for 66% of the simulation time (cf., 90% for the wild type). The residual partitioning of the scrambled M2 helix into the bilayer is perhaps not surprising since bilayer partitioning of a helix (to a first approximation) depends on its amino acid composition (98). However, self-assembly simulations using this scrambled M2 helix (carried out in the same manner as for the wild-type M2 helix) resulted in “ejection” of one of the helices to the surface of the membrane whenever an aggregate formed. Thus the CG-MD self-assembly of a stable and converged M2 helix tetrameric bundle appears to be sensitive to (large-scale) changes in the sequence the peptide used.

These studies, in a broader context, illustrate the potential for CG-MD simulations to model the second stage of membrane protein folding, namely, the self-assembly/packing together of TM α -helices. It thus extends previous CG-MD simulations of formation of dimers of glycophorin A TM helices (31), and AT-MD simulations of association of model TM helices within a bilayer environment (99,100). Taken together, these studies indicate that MD simulation may provide a valuable tool to probe the process of association of TM helices, and the nature and stability of TM helix/helix interactions within a lipid bilayer environment.

It is perhaps useful here to reflect critically on the more general applicability of CG-MD to modeling helix packing within membrane proteins. Based on experience with M2 tetramerization (this article) and glycophorin A helix dimerization (31,101), it would seem that CG-MD can be used to pack simple oligomers of relatively undistorted TM helices. However, to model the packing of more complex assemblies of TM helices, possibly including helices, e.g., kinked by the presence of proline residues (102) and interacting via side-chain-mediated H-bonds (103,104), a more complex, multiscale simulation approach is likely to be required.

It is important to examine the relationship of the CG-MD model of the M2 TM tetramer with available experimental and computational data. In terms of the mutational and re-

lated functional data, the CG-MD model is consistent in that it suggests that the key side chains (e.g., H37 and W41) are directed toward the center of the four-helix bundle.

A number of previous studies of self-assembly of the M2 tetramer (64,65) and of the stability of the related HIV Vpu channel TM helix pentamer (105) have employed MD simulations combining an atomistic protein model with a continuum model for the lipid bilayer and solvent. These simulations assumed N -fold rotational symmetry of the helix bundle. Here we relax this assumption, and the resultant simulations suggest the existence of a $2\times$ -symmetrical (closed) state. There is also some evidence for departure from exact $4\times$ rotational symmetry of the M2 channel in the recent x-ray crystallographic structure (66). Indeed, this structure seems to more closely match our model than the subsequent (exactly $4\times$ rotationally symmetric) model, D4, that was generated from the crystal structure. It is possible that such loss of symmetry would be more difficult to detect in NMR experiments. For example, the recent NMR structure (Fig. 6 D) determined in DHPC micelles was generated using C_4 rotational symmetry (67). However, the helix tilt angle in the NMR model ($\sim 15^\circ$) is close to that of the CG-MD generated model ($\sim 16^\circ$).

It is also productive to reflect on some of the limitations of the computational methodology used in this study. The CG force field employed is relatively simple, although it has been tested for membrane peptides and protein against a range of experimental data (28,30). Furthermore, this and related CG models have been used successfully to characterize the interactions of integral proteins (106) with lipid bilayers, to probe lipid bilayer deformation by integral membrane proteins (32,33), and to explore bilayer/protein coupling in gating of mechanosensitive channels (107). Refinement of the force field for lipids was recently reported (29), and this refinement has been extended to peptides and proteins (108). It will therefore be important to explore the sensitivity/robustness of our conclusions to such improvements in the CG force field.

We used our converged CG model of the M2 helix bundle as the starting point for a (brief) AT-MD simulation. Another possible means of capturing atomistic detail is to combine CG and AT components within the same simulation (25,26,109–111). Such an approach may provide a more accurate, yet still computationally feasible, route to modeling self-assembly of TM helix bundles. We also would like to explore a more sophisticated (and possibly automated (112)) approach to initiation and implementation of CG \rightarrow AT switching. For example, one might consider that an appropriate switch time would be shortly after a transition between the two $2\times$ -symmetrical bundle conformations. This can be determined by monitoring, e.g., the pattern of interhelix distances as the CG-MD simulation proceeds and thus automatically initiating the switch to AT-MD. Thus a single long (multi-microseconds) CG-MD simulation could spawn an ensemble of shorter (multi-nanoseconds) AT-MD simulations.

In terms of future directions of these studies, it will be of interest to extend the approach to self-assembly of TM helix bundles (e.g., phospholamban (J. Vorel and M. S. P. Sansom, unpublished results)), to TM helix hairpins fragments from more complex membrane proteins (28), and ultimately to multipass membrane protein helix bundles. In this way it may be possible to develop CG-MD as a component of a multi-scale approach for predicting membrane protein structure via simulation.

SUPPLEMENTARY MATERIAL

To view all of the supplemental files associated with this article, visit www.biophysj.org.

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